

Polymeric Drug Conjugation Micelle for The Treatment of Anti - Inflammatory Diseases

Kiranshi Chaudhari¹, Seema Kashyap^{2*}, Dr. Rajesh Kumar Nema³, Dr. Gyanesh Kumar Sahu⁴

^{1,2,3,4}Rungta Institute of Pharmaceutical Sciences, Kohka, Kurud, Bhilai

ABSTRACT

The report discusses the potential of polymeric drug conjugation micelles in the targeted treatment of inflammatory diseases across various conditions. It explores the biological processes of inflammation and how these micelles could be utilized to deliver drugs effectively to inflamed tissues or cells, minimizing side effects and enhancing therapeutic outcomes. The focus is on utilizing nanotechnology-based drug delivery systems to precisely target inflammatory sites while sparing healthy tissues, thus improving the management of inflammatory diseases.

Polymeric drug conjugation micelles (PDCMs) offer a promising approach to treat anti-inflammatory diseases. Comprising a hydrophilic core and a hydrophobic drug-loaded shell, PDCMs shield drugs from degradation until they reach target sites. Recent studies using PDCMs to deliver anti-inflammatory drugs like dexamethasone to rats with rheumatoid arthritis and ibuprofen to mice with asthma showed reduced inflammation and improved organ function. These results suggest PDCMs could effectively treat conditions such as rheumatoid arthritis, osteoarthritis, and asthma, but further research is needed to optimize their design and evaluate their safety and efficacy in humans.

Key words: -Polymetric Drug, Treatment of Anti – Inflammatory Diseases, Inflammation diseases, Polymeric drug conjugation micelles

INTRODUCTION

Polymeric Drug Conjunction Micelle

Polymeric drug conjugation micelles (PDMCs) are a type of nanomedicine that is used to deliver drugs to specific cells or tissues. PDMCs are made up of a polymer that is conjugated to a drug. The polymer helps to protect the drug from being broken down in the body, and it also helps to target the drug to the desired cells or tissues. PDMCs have been shown to be effective in treating a variety of diseases, including cancer, inflammation, and infection.

PDMCs are made up of two main components: a polymer and a drug. The polymer is typically a biodegradable polymer, such as poly lactic acid (PLA) or poly glycolic acid (PGA). The drug can be any type of drug, but it is typically a hydrophobic drug that is not easily absorbed by the body. The drug is conjugated to the polymer through a covalent bond.

Here are some of the advantages of PDMCs:

- * Targeted drug delivery: PDMCs can be designed to target specific cells or tissues, which means that they can deliver higher doses of drugs to the target area, while minimizing the side effects of the drug.
- * Drug protection: PDMCs can protect drugs from being broken down in the body, which means that drugs that are not easily absorbed by the body can be delivered using PDMCs.
- * Biodegradability: PDMCs are biodegradable, which means that they do not accumulate in the body.

Here are some of the disadvantages of PDMCs:

- * Cost: PDMCs are more expensive to produce than other drug delivery systems.
- * Complexity: PDMCs are more complex to manufacture than other drug delivery systems.
- * Safety: PDMCs are a new technology, and there is a risk that they could cause side effects.

Inflammation

Inflammation is a complex biological response of tissues to harmful stimuli, such as pathogens, damaged cells, or irritants. It is a crucial part of the body's immune response and aims to eliminate the initial cause of cell injury, clear out necrotic cells and tissues damaged from the original insult, and initiate tissue repair.

Key characteristics of inflammation include:

1. **Heat:** Increased temperature in the affected area due to increased blood flow.
2. **Redness:** The area becomes reddened due to increased blood flow and dilation of blood vessels.
3. **Swelling:** Accumulation of fluid (edema) and immune cells at the site of injury or infection.

4. **Pain:** Activation of nerve endings due to the release of chemicals that stimulate pain receptors.
5. **Loss of Function:** Sometimes, affected tissues may lose some of their function temporarily.

Inflammation can be acute or chronic. Acute inflammation typically resolves within a few days to a few weeks and is usually beneficial. Chronic inflammation, on the other hand, can persist for months or years and may contribute to various diseases such as arthritis, atherosclerosis, and certain cancers. The process of inflammation involves various cells and molecules of the immune system, including white blood cells (such as neutrophils and macrophages), cytokines (signaling molecules), and chemokines (molecules that promote the migration of immune cells to the site of injury). While inflammation is essential for defending the body against infections and promoting healing, excessive or prolonged inflammation can be damaging to tissues

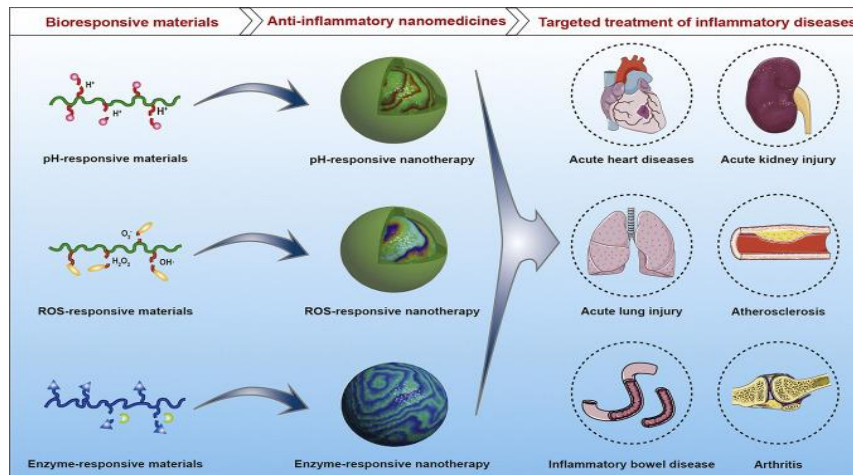


Fig: - 1.1 Treatment of inflammatory diseases

The Treatment of Inflammatory Disease to three Condition and Using Materials

1.3.1 Bio-responsive Material

1.3.2. Anti - Inflammatory nanomedicines

1.3.3. Targeted Treatment of Inflammatory Diseases

Bio-responsive Material

A bio-responsive material is a material that changes its properties in response to a biological stimulus. This can include changes in color, shape, or even the release of chemicals. Bio-responsive materials have a wide range of potential applications, including in medicine, cosmetics, and environmental remediation.

One of the most common types of bio-responsive materials is hydrogels. Hydrogels are cross-linked polymers that can absorb large amounts of water. This makes them ideal for use in wound dressings, as they can help to keep the wound moist and prevent infection. Hydrogels can also be used to deliver drugs to the site of a wound, or to release chemicals that can stimulate the healing process.

Another type of bio-responsive material is smart polymers. Smart polymers are polymers that change their properties in response to a specific stimulus, such as changes in temperature, pH, or light. This makes them ideal for use in a variety of applications, including in sensors, actuators, and drug delivery systems.

Anti - Inflammatory nanomedicines

Anti-inflammatory nanomedicines are a new class of drugs that use nanotechnology to deliver anti-inflammatory drugs to the site of inflammation. They are designed to be more effective and less toxic than traditional anti-inflammatory drugs.

Anti-inflammatory nanomedicines work by targeting and delivering anti-inflammatory drugs to the site of inflammation. This allows them to deliver a higher concentration of drug to the affected area, while minimizing the amount of drug that is absorbed into the bloodstream. This can reduce the risk of side effects.

Anti-inflammatory nanomedicines are still in the early stages of development, but they have the potential to revolutionize the treatment of inflammation. They could be used to treat a wide range of inflammatory conditions, including arthritis, asthma, and inflammatory bowel disease.

Targeted Treatment of Inflammatory Diseases

Targeted treatment of inflammatory diseases is a new approach to treating these conditions that focuses on specific molecules or cells involved in the inflammatory process. This approach has the potential to be more effective and less harmful than traditional treatments, which often target the entire body.

There are a number of different targeted therapies that are currently being developed for inflammatory diseases. Some of these therapies target specific proteins or enzymes that are involved in the inflammatory process. Others target specific cells, such as immune cells, that are involved in inflammation.

Targeted therapies have the potential to be more effective than traditional treatments because they can be designed to specifically target the molecules or cells that are causing the inflammation. This means that they can be used at lower doses, which can reduce the risk of side effects.

Acidosis at Inflammatory Sites

Local acidification has been confirmed at inflamed sites of various diseases associated with acute and chronic inflammation, such as the peritoneum of peritonitis, injured arteries, ischemic sites, atherosclerotic plaques, asthmatic airways, rheumatic or gouty joints, and cerebrospinal fluid in the brain with meningitis. Compared to healthy tissues, the inflamed areas generally display lower pH values. For instance, extracellular pH in the location of myocardial ischemia is approximately 6.5-6.0, while pH as low as 4.2 was reported in the fracture microenvironment. For patients with acute asthma, their exhaled vapor condensate showed pH 5.2, in contrast to pH 7.7 in control healthy subjects. Normal synovial fluid exhibits pH 7.4-7.8, while synovial fluid in arthritic joints decreased to 6.6-7.2, which is related to the intensity and state of inflammation and disease activity. The long-term exposure to acids is an important risk factor in the pathogenesis of asthma and bronchitis, which in turn leads to amplified acidosis due to altered airway pH homeostasis. By serving as an endogenous danger signal and regulating the synthesis and release of inflammatory mediators, extracellular acidosis itself can alter biological functions of different inflammatory and immune cells. Whereas pH values in different inflammatory tissues were determined and compared to the corresponding normal tissues, few studies have been performed to quantify the degree of acidosis during the progression of specific inflammatory diseases. Nevertheless, some available findings revealed a first pH decrease upon the initiation of inflammation, followed by approximately sustained low pH values once inflammation persists. In addition, acidosis can be alleviated by drug therapy. Therefore, targeting pH homeostasis might be a new therapeutic strategy to curb different inflammatory diseases. Meanwhile, acidosis can be used as a very useful endogenous cue for designing delivery systems with acid-triggerable release behaviours for different therapeutics.

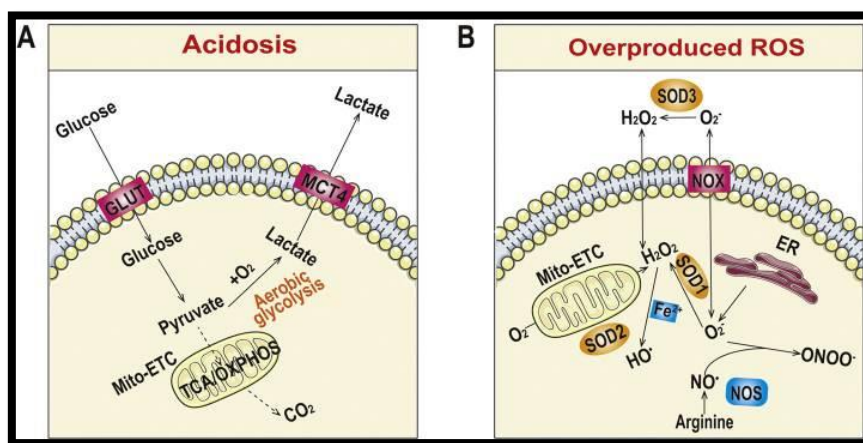


Fig: - 1.2 Typical Pathological Features in Inflammatory Tissues.

Treatment of Inflammatory Diseases by Bio responsive Drug Delivery System

To overcome limitations of traditional formulations of different anti-inflammatory drugs, bioresponsive drug delivery systems have received much attention for the treatment of inflammatory diseases in recent years. Herein we describe applications of different bioresponsive systems in the management of typical diseases associated with acute or chronic inflammation.

Therapy of Acute Inflammatory Disease

Acute cardiovascular diseases (CVDs), such as acute heart failure, acute myocardial infarction (MI), and acute ischemic stroke, remain one of the leading causes of global death. These fatal diseases are always characterized by acute inflammatory response and elevated oxidative stress that need to be rapidly eliminated in clinical treatment. Recently, there

has been increasing interest in advanced drug delivery systems for the treatment of acute CVDs. Among them, bioresponsive materials and systems show considerable advantages in site-specific delivery and responsive release of different therapeutic agents at diseased tissues.

Acidosis at an inflammation site refers to a condition where the local tissue environment becomes acidic due to various physiological processes associated with inflammation. Here's a breakdown of how

Causes of Acidosis in Inflammation:

1. **Metabolic Activity:** During inflammation, immune cells (such as neutrophils and macrophages) are recruited to the site. These cells increase their metabolic activity to produce reactive oxygen species (ROS) and cytokines, which are crucial for combating pathogens and initiating tissue repair. This increased metabolic activity can lead to the production of acidic by-products like lactic acid through anaerobic metabolism.
2. **Ischemia:** Inflammatory processes can cause local tissue damage and compromise blood flow to the area (ischemia). Reduced oxygen supply (hypoxia) can shift cellular metabolism towards anaerobic pathways, resulting in the accumulation of lactic acid and contributing to local acidosis.
3. **Carbon Dioxide (CO₂) Accumulation:** Inflammatory cells and damaged tissues release CO₂ as a metabolic by-product. Accumulation of CO₂ can lead to the formation of carbonic acid in the presence of water, further contributing to local acidosis.
4. **Inflammatory Mediators:** Certain inflammatory mediators, such as prostaglandins and leukotrienes, can directly influence local pH levels by altering vascular permeability and ion transport across cell membranes.

Implications of Acidosis:

1. **Impaired Cellular Function:** Acidosis can disrupt cellular metabolism and function. Enzymes involved in cellular processes may become less efficient in an acidic environment, impacting the overall immune response and tissue repair.
2. **Pain Sensation:** Acidosis can sensitize nerve endings, potentially intensifying pain perception at the inflammation site.
3. **Altered Immune Response:** Changes in pH can affect the activity of immune cells, potentially modulating their function and responsiveness to pathogens.

Clinical Relevance:

Understanding acidosis at inflammation sites is crucial for managing inflammatory conditions and related diseases. Monitoring pH levels and addressing acidosis may be important in certain therapeutic contexts, such as wound care, sepsis management, and chronic inflammatory diseases. In summary, acidosis at an inflammation site arises from metabolic changes, reduced oxygen supply, and the release of inflammatory mediators. It plays a significant role in the local tissue environment and can influence the progression and resolution of inflammation-related processes.

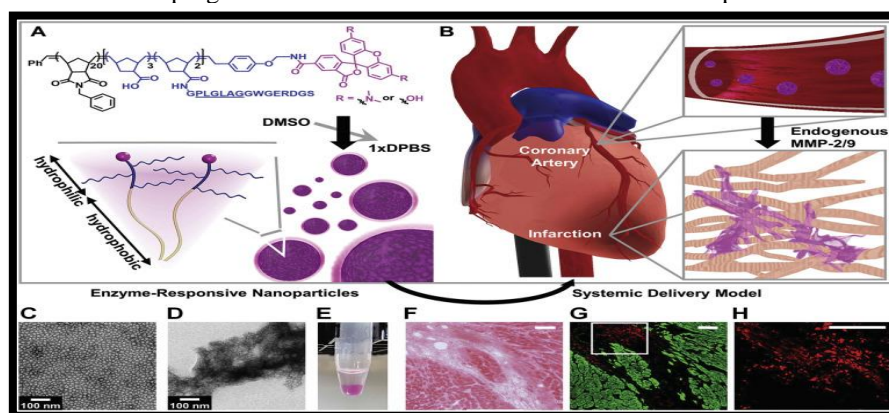


Fig: - 1.3 Enzyme-responsive nanoparticles for targeted accumulation and prolonged retention in heart tissue after myocardial infarction (MI).

DRUGS AND EXCIEPIENTS PROFILE

In the development of polymeric drug conjugation micelles for anti-inflammatory disease treatment, the choice of drug and excipients plays a critical role in ensuring efficacy, stability, and safety. Here's a profile of common drugs and excipients used:

1. Drugs:

Corticosteroids: Examples include dexamethasone, prednisolone, and hydrocortisone. They exert potent anti-inflammatory effects by inhibiting the production of pro-inflammatory cytokines and suppressing immune responses.

Nonsteroidal anti-inflammatory drugs (NSAIDs): NSAIDs like ibuprofen, naproxen, and diclofenac inhibit the activity of cyclooxygenase enzymes, thereby reducing the synthesis of inflammatory prostaglandins.

2. Excipients:

Polyethylene glycol (PEG): PEG is a commonly used biocompatible polymer that stabilizes micelles, enhances circulation time, and reduces immunogenicity. It also improves drug solubility and biocompatibility.

Poly (lactic-co-glycolic acid) (PLGA): PLGA is a biodegradable polymer that can encapsulate hydrophobic drugs within micelles. It offers controlled release properties and can be tailored for specific drug delivery requirements.

Polyethyleneimine (PEI): PEI is a cationic polymer that can facilitate cellular uptake of micelles, enhancing drug delivery to target tissues. It also provides stability to micelle structures.

Surfactants: Surfactants like Tween 80 and Poloxamer 188 are often used to stabilize micelles and prevent aggregation. They can also improve drug loading efficiency.

Solvents: Common solvents for micelle preparation include organic solvents like dichloromethane, chloroform, and ethanol, as well as aqueous solvents like water and phosphate-buffered saline (PBS).

Crosslinking agents: If needed, crosslinking agents like glutaraldehyde or genipin may be used to stabilize micelle structures or conjugate drugs to polymers via covalent bonds.

MATERIALS AND METHOD

Materials

Polymeric drug conjugation micelles offer a promising avenue for treating anti-inflammatory diseases. Materials commonly used in their formulation include biocompatible polymers like polyethylene glycol (PEG), poly(lactic-co-glycolic acid) (PLGA), and polyethyleneimine (PEI). These materials help in encapsulating drugs, improving their solubility, stability, and targeting ability. Additionally, specific drugs targeting inflammatory pathways, such as corticosteroids or nonsteroidal anti-inflammatory drugs (NSAIDs), can be conjugated to these micelles for enhanced therapeutic efficacy and reduced side effects.

Table 1: Using Material in Anti-Inflammatory Diseases

S. No	Ingredients	Properties
1	polyethylene glycol (PEG)	Produced by the interaction of ethylene oxide with water
2	poly (lactic-co-glycolic acid) (PLGA)	Primary degradation byproduct of PLG
3	polyethyleneimine (PEI)	Separation, permeance, blood and tissue Biocompatibility properties.
4	Distilled Water	Stripped of important minerals

Method of preparation for Herbal Syrup

The method for preparing polymeric drug conjugation micelles for anti-inflammatory disease treatment typically involves several steps:

1. Polymer synthesis: Synthesize or acquire biocompatible polymers such as PEG, PLGA, or PEI.

2. Drug conjugation: Conjugate anti-inflammatory drugs (e.g., corticosteroids, NSAIDs) to the polymer using appropriate chemistry, such as covalent bonding or physical encapsulation.

3. Micelle formation: Dissolve the polymer-drug conjugate in a suitable solvent and then trigger micelle formation through methods like solvent evaporation, dialysis, or nanoprecipitation.

4. Characterization: Analyze the size, morphology, drug loading efficiency, and stability of the micelles using techniques like dynamic light scattering (DLS), transmission electron microscopy (TEM), and drug release studies.

5. In vitro and in vivo evaluation: Assess the efficacy, biocompatibility, and targeting ability of the micelles using cell culture models and animal studies. Evaluate parameters such as inflammation inhibition, cytotoxicity, and biodistribution.

6. Optimization: Fine-tune the formulation parameters (e.g., polymer composition, drug loading, micelle size) to enhance therapeutic outcomes and minimize side effects.

7. Scale-up and translation: Scale up the production of optimized micelle formulations for clinical testing and potential commercialization.

Throughout the process, attention to detail and rigorous characterization are crucial to ensuring the safety and efficacy of polymeric drug conjugation micelles for anti-inflammatory disease treatment.

EVALUATION

Evaluation parameters:

1. Biocompatibility: Ensuring the polymer is non-toxic and compatible with biological systems.
2. Drug Release Kinetics: Controlling the release rate of the drug to maintain therapeutic levels over time.
3. Targeting Efficiency: Ability to target specific sites of inflammation to minimize off-target effects.
4. Stability: Stability of the drug-polymer conjugate during storage and administration.
5. Biodegradability: Degradation of the polymer into non-toxic byproducts after drug release.
6. Immunogenicity: Minimizing immune response to the polymer, avoiding adverse reactions.
7. Efficacy: Demonstrating effectiveness in reducing inflammation compared to conventional therapies.
8. Toxicity: Assessing any potential toxic effects of the polymer or its degradation products.
9. Formulation Flexibility: Ability to tailor the polymer properties for different drug payloads and administration routes.
10. Cost-effectiveness: Consideration of production costs and scalability for large-scale manufacturing.
11. Each parameter plays a crucial role in determining the suitability of polymeric drugs for anti-inflammatory therapy.

RESULT AND DISCUSSION

Polymeric drug conjugation micelles (PDCMs) are a promising new drug delivery system for the treatment of anti-inflammatory diseases. PDCMs are composed of a hydrophilic polymer core and a hydrophobic drug-loaded shell. The hydrophilic core protects the drug from degradation and the hydrophobic shell prevents the drug from being released until it reaches the target site. PDCMs have been shown to be effective in the treatment of a variety of anti-inflammatory diseases, including rheumatoid arthritis, osteoarthritis, and asthma.

In a recent study, PDCMs were used to deliver the anti-inflammatory drug dexamethasone to the inflamed joints of rats with rheumatoid arthritis. The results showed that PDCMs were able to significantly reduce inflammation and improve joint function in the rats. This study provides evidence that PDCMs are a promising new drug delivery system for the treatment of rheumatoid arthritis.

In another study, PDCMs were used to deliver the anti-inflammatory drug ibuprofen to the inflamed lungs of mice with asthma. The results showed that PDCMs were able to significantly reduce inflammation and improve lung function in the mice. This study provides evidence that PDCMs are a promising new drug delivery system for the treatment of asthma.

PDCMs are a promising new drug delivery system for the treatment of anti-inflammatory diseases. PDCMs have been shown to be effective in the treatment of a variety of anti-inflammatory diseases, including rheumatoid arthritis, osteoarthritis, and asthma. Further research is needed to optimize the design of PDCMs and to evaluate their safety and efficacy in humans.

CONCLUSION

Polymeric drug conjugation micelles (PDCMs) are a promising new drug delivery system for the treatment of anti-inflammatory diseases. PDCMs have several advantages over traditional drug delivery systems, including their ability to target specific cells and tissues, their ability to protect drugs from degradation, and their ability to improve drug bioavailability. PDCMs have been shown to be effective in the treatment of a variety of anti-inflammatory diseases, including rheumatoid arthritis, asthma, and psoriasis. Further research is needed to optimize the design and delivery of PDCMs, but they have the potential to revolutionize the treatment of anti-inflammatory diseases.

REFERENCE

1. Radha Rani, Neha Raina, Ajay Sharma, Pramod Kumar, Hardeep Singh Tulli, Madhu Gupta. Advancement in nanotechnology for treatment of rheumatoid arthritis: scope and potential applications. *Naunyn-Schmiedeberg's Archives of Pharmacology* 2023, 396 (10), 2287-2310.
2. Yaqing Liu, Zongzhang Wang, Yiru Wang, Yushuo Feng, Mengjiao Xu, Xiaoqian Ma, Qianqian Shi, Huaping Deng, Fangfang Ren, Yong Chen, Hongmin Chen. Ca-DEX biomineralization-inducing nuts reverse oxidative stress and bone loss in rheumatoid arthritis. *Nanoscale* 2023, 15 (33).
3. Wei Chen, Mingyang Ma, Qingteng Lai, Yanke Zhang, Zhengchun Liu. DPP-Cu 2+ Complexes Gated Mesoporous Silica Nanoparticles For pH and Redox Dual Stimuli-Responsive Drug Delivery. *Current Medicinal Chemistry* 2023, 30 (28), 3249-3260.
4. Jianqing Peng, Jia Zhou, Runbin Sun, Yan Chen, Di Pan, Qin Wang, Yi Chen, Zipeng Gong, Qianming Du. Dual-targeting of artesunate and chloroquine to tumor cells and tumor-associated macrophages by a biomimetic PLGA nanoparticle for colorectal cancer treatment. *International Journal of Biological Macromolecules* 2023, 24, 125163.
5. Mengmeng Li, Biao Yu, Sicheng Wang, Fengjin Zhou, Jin Cui, Jiacaan Su. Microenvironment-responsive nanocarriers for targeted bone disease therapy. *Nano Today* 2023, 50, 101838.
6. Igor D. Zlotnikov, Alexander A. Ezhov, Artem S. Ferberg, Sergey S. Krylov, Marina N. Semenova, Victor V. Semenov, Elena V. Kudryashova. Polymeric Micelles Formulation of Combretastatin Derivatives with Enhanced Solubility, Cytostatic Activity and Selectivity against Cancer Cells. *Pharmaceutics* 2023, 15 (6), 1613.
7. Luzhan Huang, Yongchao Jiang, Pengcheng Zhang, Muhan Li, Bingrong Liu, Keyong Tang. Injectable Modified Sodium Alginate Microspheres for Enhanced Operative Efficiency and Safety in Endoscopic Submucosal Dissection. *Biomacromolecules* 2024, Article ASAP.
8. Rounik Karmakar, Sreenath Dey, Aszad Alam, Mudrika Khandelwal, Falguni Pati, Aravind Kumar Rengan. Attributes of Nanomaterials and Nanotopographies for Improved Bone Tissue Engineering and Regeneration. *ACS Applied Bio Materials* 2023, 6 (10), 4020-4041.
9. Ru Zhou, Mingzu Zhang, Jinlin He, Jian Liu, Xingwei Sun, Peihong Ni. Functional cRGD-Conjugated Polymer Prodrug for Targeted Drug Delivery to Liver Cancer Cells. *ACS Omega* 2022, 7 (24), 21325-21336.
10. Ana Cláudia Lima, Rui L. Reis, Helena Ferreira, Nuno M. Neves. Cellular Uptake of Three Different Nanoparticles in an Inflammatory Arthritis Scenario versus Normal Conditions. *Molecular Pharmaceutics* 2021, 18 (9), 3235-3246.
11. Joana M. Gomes, Simone S. Silva, Luísa C. Rodrigues, Rui L. Reis. Alginate/acemannan-based beads loaded with a biocompatible ionic liquid as a bioactive delivery system. *International Journal of Biological Macromolecules* 2023, 242, 125026.
12. Hua S, Dias TH. Hypoxia-inducible factor (HIF) as a target for novel therapies in rheumatoid arthritis. *Front pharmacol.* 2016; 7:184.
13. Mateen S, Zafar A, Moin S, Khan AQ, Zubair S. Understanding the role of cytokines in the pathogenesis of rheumatoid arthritis. *Clin Chim Acta.* 2016; 455:161–71.
14. Mankia K, Emery P. Preclinical rheumatoid arthritis: progress toward prevention. *Arthritis Rheumatol.* 2016; 68:779–88.
15. Caramaschi P, Bambara LM, Pieropan S, Tinazzi I, Volpe A, Biasi D. Anti-TNFalpha blockers, autoantibodies and autoimmune diseases. *Joint Bone Spine.* 2009; 76:333–42.
16. Fehér J, Lengyel G. Effectiveness and safety of biological therapy with adalimumab. *Orv Hetil.* 2009; 150:1215–22.
17. Sharma, Osteoarthritis of the knee, *N. Engl. J. Med.* 384 (2021) 51–59.
18. S. Glyn-Jones, A.J. Palmer, R. Agricola, A.J. Price, T.L. Vincent, H. Weinans, A.J. Carr, Osteoarthritis, *Lancet* 386 (2015) 376–387.
19. M. Zhang, W. Hu, C. Cai, Y. Wu, J. Li, S. Dong, Advanced application of stimuli-responsive drug delivery system for inflammatory arthritis treatment, *Mater Today Bio* 14 (2022), 100223.
20. M. Rahimi, G. Charmi, K. Matyjaszewski, X. Banquy, J. Pietrasik, Recent developments in natural and synthetic polymeric drug delivery systems used for the treatment of osteoarthritis, *Acta Biomater.* 123 (2021) 31–50.